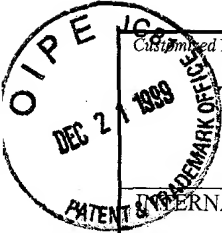


416 Rec'd PCT/PTO

21 DEC 1999

PCT



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U.S. DEPARTMENT OF COMMERCE PATENT AND TRADEMARK OFFICE

ATTORNEY DOCKET NO.

P06597US0/MP

**TRANSMITTAL LETTER TO THE UNITED STATES  
DESIGNATED/ELECTED OFFICE (DO/EO/US)  
CONCERNING A FILING UNDER 35 U.S.C. 371**

09/446379

INTERNATIONAL APPLICATION NO.  
PCT/GB98/01882INTERNATIONAL FILING DATE  
26 JUNE 1998PRIORITY DATE CLAIMED  
26 JUNE 1997

TITLE OF INVENTION: CELL CULTURE PRODUCTS

APPLICANT(S) FOR DO/EO/US: THOMSON, Brian M. et al.

Applicant herewith submits to the US Designated/Elected Office (DO/EO/US) the following items and other information:

- ☒ 1. This is a **FIRST** submission of items concerning a filing under 35 U.S.C. 371.
- ☐ 2. This is a **SECOND** or **SUBSEQUENT** submission of items concerning a filing under 35 USC 371.
- ☒ 3. This express request to begin national examination procedures (35 USC 371(f)) at any time rather than delay examination until the expiration of the applicable time limit set in 35 USC 371(b) and PCT Art. 22 and 39(1).
- ☒ 4. A proper Demand for International Preliminary Examination was made by the 19<sup>th</sup> month from the earliest claimed priority date.
- ☒ 5. A **copy** of the International Application as filed (35 U.S.C. 371 (c)(2))
  - ☐ a. is transmitted herewith (required only if not transmitted by the International Bureau).
  - ☒ b. has been transmitted by the International Bureau.
  - ☐ c. is not required, as the application was filed in the United States Receiving Office (RO/US).
- ☐ 6. A **translation** of the International Application into English (35 U.S.C. 371(c)(2)).
- ☒ 7. Amendments to the claims of the International Appln. under PCT Article 19 (35 USC 371 (c)(3))
  - ☐ a. are transmitted herewith (required only if not transmitted by the International Bureau).
  - ☐ b. have been transmitted by the International Bureau.
  - ☐ c. have not been made; however, the time limit for making such amendments had NOT expired.
  - ☒ d. have not been made and will not be made.
- ☐ 8. A translation of the amendments to the claims under PCT Article 19 (35 U.S.C. 371(c)(3)).
- ☐ 9. An **oath** or declaration of the inventor(s) (35 U.S.C. 371(c)(4)).
- ☐ 10. A translation of the annexes to the International Preliminary Examination Report under PCT Article 36 (35 U.S.C. 371(c)(5)).

**Items 11. to 16. below concern document(s) or information included:**

- ☐ 11. An **Information Disclosure Statement** under 37 C.F.R. 1.97 and 1.98.
- ☐ 12. An **Assignment** document for recording. A separate cover sheet in compliance with 37 CFR 3.28 and 3.31 is included.
- ☒ 13. A **First preliminary amendment**.
  - ☐ A Second or subsequent preliminary amendment.
- ☐ 14. A substitute specification.
- ☐ 15. A change of power of attorney and/or address letter.
- ☐ 16. Other items or information:
  - ☐ **Small Entity Statement**
  - ☐
- ☐ A copy of the Notification of Missing Requirements under 35 U.S.C. 371.
- ☐ In the event that a petition for extension of time is required to be submitted herewith, and in the event that a separate petition does not accompany this response, applicant hereby petitions under 37 CFR 1.136(a) for an extension of time of as many months as are required to render this submission timely. Any fee is authorized in 17(c).

Date: 21 Dec. 1999

09/446379

416 Rec'd PCT/PTO 21 DEC 1999

INTERNATIONAL APPLICATION NO. PCT/GB98/01882		INTERNATIONAL FILING DATE 26 JUNE 1998		PRIORITY DATE CLAIMED 26 JUNE 1997	
<input checked="" type="checkbox"/> 17. The following fees are submitted: <input checked="" type="checkbox"/> <b>Basic National Fee</b> (37 CFR 1.492 (a) (1)-(5):					
<input checked="" type="checkbox"/> Search Report has been prepared by the EPO or JPO \$ 840 <input type="checkbox"/> International preliminary examination fee paid to USPTO \$ 670 <input type="checkbox"/> No Int'l Prelim. Ex. fee paid to USPTO but Int'l Search fee paid to USPTO \$ 760 <input type="checkbox"/> Neither Int'l Prelim. Exam. fee nor Int'l Search fee paid to USPTO \$ 970 <input type="checkbox"/> Int'l Prelim. Ex. fee paid to USPTO & all claims satisfied PCT Art. 33(1)-(4) \$ 96					
ENTER APPROPRIATE BASIC FEE AMOUNT =				\$840.00	
<input type="checkbox"/> Surcharge of \$130 for furnishing the oath or declaration later than from the earliest claimed priority date (37 CFR 1.492(e)).				<input type="checkbox"/> 20 mos. <input type="checkbox"/> 30 mos. +	\$
CLAIMS	NUMBER FILED	NUMBER EXTRA	RATE		
Total Claims	17 - 20 =		X \$18 =	\$	
Independent Claims	4 - 03 =	1	X \$78 =	\$ 78.00	
<input type="checkbox"/> Multiple Dependent Claim(s) (if applicable)			+ \$260 =	\$	
TOTAL OF ABOVE CALCULATIONS =				\$ 918.00	
<input type="checkbox"/> Reduction of 1/2 for filing by small entity, if applicable. Small Entity Statement must also be filed.				\$	
SUBTOTAL =				\$ 918.00	
<input type="checkbox"/> Processing fee of \$130 for furnishing the English translation later than from the earliest claimed priority date (37 CFR 1.492(f)).				<input type="checkbox"/> 20 mos. <input type="checkbox"/> 30 mos. +	\$
TOTAL NATIONAL FEE =				\$ 918.00	
<input type="checkbox"/> Fee for recording the enclosed assignment, accompanied by a cover sheet - \$40 per property				\$	
TOTAL FEES ENCLOSED =				\$ 918.00	
Amount to be				Refunded	\$
				Charged	\$
<input checked="" type="checkbox"/> a. A check in the amount of \$918.00 to cover the above fees is enclosed. <input type="checkbox"/> b. Please charge my Deposit Account No. 12-0555 in the amount of \$ to cover the above fees. <input checked="" type="checkbox"/> c. The Commissioner is hereby authorized to charge any additional fees required or credit overpayment to Deposit Account No. 12-0555.					
<b>Note:</b> Where an appropriate time limit under 37 CFR 1.494 or 1.495 has not been met, a petition to revive (37 CFR 1.137(a) or (b)) must be filed and granted to restore the application to pending status.					
Address correspondence to: <b>MARVIN PETRY</b> At the address (below) of <b>CUSTOMER NO. 000881.</b>  <b>LARSON &amp; TAYLOR, PLC</b> <b>1199 NORTH FAIRFAX ST.</b> <b>SUITE 900</b> <b>ALEXANDRIA, VA 22314</b>			SIGNATURE: <u>Douglas E. Jackson</u> NAME: DOUGLAS E. JACKSON REG. NO.: 28518 PHONE NO.: 703-739-4900		
			Date: 21 DEC 1999		

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IN THE UNITED STATES PATENT AND TRADEMARK OFFICE

Patent

In re application of THOMSON ET AL )  
New Application ) Atty's Dckt: P06597USO/MP  
Filed: On even date herewith ) Application Branch  
For: CELL CULTURE PRODUCTS )

PRELIMINARY AMENDMENT

Hon. Assistant Commissioner of Patents  
Washington, D.C. 20231

S I R:

Preliminary to the examination thereof, please amend the above-identified application as follows:

IN THE CLAIMS:

Claim 6, line 1, delete "or 5".

Claim 7, line 1, delete "any one preceding claim", and insert therefor --claim 1--.

Claim 9, line 1, delete "or 8".

Claim 10, line 1, delete "any of claims 1 to 6", and insert therefor --claim 1--.

Claim 12, line 1, delete "any preceding claim", and insert therefor --claim 1--.

Claim 15, line 1, delete "claims 12 to 14", and insert therefor --claim 12--.

Claim 16, line 1, delete "claims 12 to 14", and insert therefor --claim 12--.

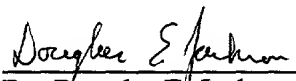
REMARKS

The above amendments are being made in order to place the application in better condition for examination and to reduce the filing fee.

Favorable consideration is respectfully requested.

Respectfully submitted,

Date: 12/21/1999

  
By: Douglas E. Jackson  
Registration No. 28518

**LARSON & TAYLOR**

1199 North Fairfax Street, Ste. 900 • Alexandria, Virginia 22314 • (703) 739-4900

09/446379

CELL CULTURE PRODUCTS

5 The present invention relates to the culturing of mammalian anchorage dependent cells onto a carrier substrate. More particularly, the present invention relates to wound dressings suitable for treating e.g. partial thickness wounds such as burns or skin graft donor site and to systems for the preparation of such dressings.

10 The current widely practised approach to the treatment of severe skin trauma necessitates the removal of dead tissue which might otherwise support the proliferation of pathogenic micro-organisms. However, this procedure often leaves massive open wounds which require closure and the use of autologous skin grafts  
15 is not particularly desired for a number of reasons, not least because there may be, in cases of serious burns for example, a limited supply of unaffected tissue. Cadaver skin grafts have been used to temporarily close a wound site but its limited supply and the perceived concern with cross-contamination with bacterial or viral  
20 pathogens has led to a search for alternatives.

In recent years, techniques for the *in vitro* cultivation of keratinocytes from human epidermis have been developed for culturing on epidermal sheets to cover full thickness burns. In the  
25 earliest versions of this approach, a confluent usually multilayered keratinocyte sheet was grown on tissue culture plastic *in vitro*. The cell layer would then be detached from the culture plastic using degradative enzymes, inverted and placed upon the wound. Reports on the efficiency of this approach indicate that substantial  
30 practical difficulties exist (see, for example, J Burn Care Rehab. 13, 174-180).

More recently keratinocytes have been cultured on flexible, biocompatible membranes to facilitate the transfer of cell sheets onto the wound site. See for example, our patent application

5 WO91/13638. Other illustrative examples of this approach include those disclosed in WO88/08448, EP 0364306, EP 0387975 and US 5266480. One difficulty with prior art approaches is that the use of membranes optimised for keratinocyte attachment thereto during the culturing phase can often inhibit the migration of the cells from the

10 membrane onto the wound, following the application of the wound dressing. Indeed, the prior art has tended to concentrate on improving the attachment of cells to the membrane, see for example US 5,558,861 where the use of microbially produced cellulose is disclosed having an animal cell adhesive protein physically or

15 chemically bonded thereto, the express aim of which is to provide a cellulose gel having an excellent adhesion to epidermal cells.

It is therefore an object of the present invention to provide a wound dressing which comprises a carrier layer that promotes the

20 culturing and anchoring of anchorage dependent cells *in vitro* thereto yet following application to a wound, the dressing becomes substantially non-adherent to cells.

In accordance therefore with the present invention provides a

25 wound dressing comprising a carrier layer having a wound-facing surface, said surface being non-adherent to anchorage-dependent cells and having disposed thereon a biodegradable cell anchoring layer.

30 By the term "biodegradable cell anchoring layer" we mean a layer, capable of anchoring cells thereto, that is susceptible to

degradation or breakdown following application of the dressing to the wound.

It is preferred that the dressing is conformable i.e the dressing will conform to changes in contours of the body portion to which the dressing is applied.

In preferred embodiments the carrier layer is in the form of a gel, e.g. hydrogel, a film or sheet. A film is particularly preferred. Films suitable as the carrier layer may be continuous or apertured e.g formed into a net. The film may be flat or contoured. The contours may be produced for example by embossing. Suitably contoured films may also have apertures.

The carrier layer may comprise a material which is inherently non-adherent to cells or alternatively the material may be surface treated e.g coated, with a non-adherent to cell material, to provide a carrier layer having a non-adherent to cell wound facing surface. It is observed that when a material is non-adherent to cells, the cells when suspended in a suitable aqueous medium in contact with the non-adherent material appear rounded up and do not attach to the material. In contrast, where a material is adherent to cells, the cells will attach to the material and "sit down". Furthermore, the cells will resist detachment when washed gently with physiological compatible saline.

Useful materials that are non-adherent to cells include cross-linked cellulose derivatives. Preferred examples thereof include cross-linked hydroxyalkyl celluloses e.g. hydroxyethyl cellulose, hydroxypropyl cellulose, methyl, ethyl and methylethyl celluloses (available from Sigma Co and Aldrich). Cross-linked carboxyalkyl

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- celluloses are also preferred e.g. carboxymethyl cellulose (CMC, available from Hercules Ltd, Lancashire, UK) cross-linked with ethylene glycol diglycidyl ether (EGDGE) or 1,4 butanediol diglycidyl ether. Other preferred materials include polyvinyl alcohol (PVA, Sigma Co), Cell-Form™ (ICN), agarose e.g Sepharose™.

- Alternatively a material which is adherent to cells maybe surface treated e.g by coating or by chemical/physical bonding with a non-adherent to cell material so as to provide a carrier layer having a non-adherent to cell wound facing surface. Illustrative examples of adherent materials employed in the present invention include polymers, particularly synthetic polymers, such as those disclosed in our patent applications WO 91/13638 and WO 97/06835. Apt polymers therefore include
- polyhydroxyethylmethacrylic acid (polyHEMA), cross linked polyvinylalcohol (PVA), polyacrylic acid cross linked with triallylsucrose (Carbopol), polyvinylpyrrolidone, polyetherpolyesters, polyetherpolyamides, polyacrylamides and polyethylene oxide and polyurethanes. Other apt polymers include copolymers such as those containing vinyl acetate residues such as ethylene-vinyl acetate copolymers. Suitable ethylene-vinyl acetate copolymers are those containing not more than 20% vinyl acetate. A preferred material, known as EVA 538/539 contains 16% vinyl acetate. Other suitable polymers include essentially hydrocarbon based materials such as polybutadienes, polypropylene and polystyrene. Further examples include block copolymers having hard end blocks and softer mid blocks. Apt block copolymers include styrene based rubbers such as styrene-butadiene styene (manufactured under the trade name CARIFLEX or KRATON, Shell chemical Co). The adherent material may then be coated on the wound facing surface

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with phospholcholine, or silicone, polyethylene glycol or polytetrafluoroethylene (PTFE).

The carrier layer may comprise a material which is

5 biodegradable or non-biodegradable following application of the dressing to the wound site. Illustrative examples of biodegradable materials include photopolymerizable hydrogels such as those disclosed in US 5,410,016, incorporated herein by reference, and sold under the trade name FOCAL (Focal Inc, USA).

10

The carrier layer may also comprise a backing layer disposed on a non-wound facing surface to increase the robustness of the wound dressing. Accordingly, the wound dressing may comprise a carrier layer in the form of a laminate film comprising a carrier layer

15 described hereinbefore having a backing layer disposed on a non wound-facing surface. The backing layer may be fabricated from materials commonly used in the manufacture of wound dressings such as polypropylene, polyurethanes, polyesters and polyethylene. Particular preferred are polyurethanes. Preferred polyurethane

20 backing layers include cyclic polyether polyurethanes, ESTANE 5714™ (BF Goodrich) OPSITE IV3000™ hydrophilic polyurethane film (Smith & Nephew). Polyurethane backing layers may be chemically modified with treatments such as plasma treatment with nitrogen, ammonia or air, corona discharge treatment or flame

25 treatment to increase the surface energy of the surface of the backing layer which contacts the non wound facing surface. This aims to enhance the wettability of the backing layer and thereby improve the interface between the backing layer and non wound facing surface.

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It is preferred that the carrier layer is sterilised by any suitable known methods of sterilisation. Suitable forms of sterilisation include ethylene oxide (allowing the required time for degassing), gamma-irradiation or steam sterilisation.

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It is preferred that the carrier layer is permeable to wound exudate so as to prevent the build-up of exudate under the wound dressing which might lead to the lifting or arching of the dressing away from the wound site and therefore reducing the effective contact area of the dressing with the wound site.

10

This permeability may be achieved by rendering the carrier layer sufficiently porous to wound exudate. Such rendering is standard practice in the art. Suitably, the carrier layer is permeable to moisture vapour, oxygen and carbon dioxide. In this way a dressing when in place on the wound will provide moist conditions allowing for the cells to remain viable while the wound heals and prevent the accumulation of wound exudate. It is preferred that the wound dressing of the present invention has a minimum moisture vapour transmission rate (MVTR) of around 250 to 300g/m<sup>2</sup>.

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20

The biodegradable cell anchoring layer preferably anchors the cells through attaching to the carrier layer an animal cell adhesion protein, the protein being capable of anchoring cells. According to this approach, the cell anchoring layer preferably comprises a natural or synthetic polyanion. Preferred natural polyanions include heparans, for example, heparin, heparin sulphate, fucoidin, (available from Sigma Co) syndecan, betaglycan and perlecan.

Other preferred natural polyanions include inositol phosphates e.g. inositol hexaphosphate, dextran sulphate, pentosan and

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mesoglycans (available from Sigma Co). A synthetic polyanion such as polyvinyl sulphate ( available from Sigma Co) may be used.

The polyanion is preferably cross-linked to bind the polyanion to the carrier layer. This may be achieved by the addition of an effective amount of a cross-linking agent e.g. EGDGE. It is preferred that a polyanion is utilised due to its non-specific binding properties with respect to animal cell adhesion proteins. That is, polyanions are capable of binding a large variety of animal cell adhesion proteins. As a result, the cell anchoring layer having a variety of animal cell adhesion proteins attached thereon is capable of anchoring more cells since it increases the probability that the cells will be expressing at least one factor capable of being anchored to at least one type of animal cell adhesion protein. Furthermore, polyanions bind growth factors, e.g. epidermal cell growth factors for example fibroblast growth factor (FGF). Therefore, advantageously, this promotes the formation of an engraftable cell layer. A source of cell adhesion proteins comprising a multitude of different cell adhesion proteins is preferred. Foetal calf serum (FCS) is a preferred source. Alternative sources to FCS include defined and recombinantly derived protein mixtures.

Preferably, to form the biodegradable anchoring layer, the polyanion is first made up into aqueous solution and maybe either spread on or sprayed onto the non-adherent to cell layer and allowed to dry. The polyanion may then be cross-linked as described hereinbefore.

Alternatively the cell anchoring layer may anchor the cells 'directly', that is, without the use of adhesion proteins. Short specific peptides e.g. RGD, YIGSR (available from Sigma Co) may be grafted onto non-adherent to cell layer. Other protein and peptides  
5 such as those found in soya protein may be used.

Alternatively, a polycationic peptide may anchor the cell directly. An example of which is polylysine (Sigma Co). An advantage of these direct methods is that they obviate the need to  
10 use adhesion proteins, particularly those derived from bovine sources, which would come into contact with a wound during use of the dressing.

15 The cells of the present invention are preferably mammalian epithelial or mesenchymal cells e.g. keratinocytes or fibroblasts (including precursors thereto). Melanocytes in co-culture with keratinocytes may also be used. It is preferred for burn and chronic wounds that keratinocytes are used. Preferably the keratinocytes  
20 are autologous cells, harvested according to standard techniques of the art.

Alternatively, a mixture of autologous and allogenic cells could be utilised with the present invention. In particular, where the main  
25 clinical concern is rapid closure of a dermal wound, a wound dressing according to the present invention comprising e.g. 90% allogenic keratinocytes and 10% autologous keratinocytes may be provided. The aim of which is to produce rapid wound closure following the application of the dressing. Following which, the  
30 autologous cells will progressively repopulate the wound site as the allogenic cells are rejected.

In a further alternative embodiment, the wound dressing of the present invention may comprise a mixture of keratinocytes and fibroblasts. It has been shown that the addition of fibroblasts to  
5 keratinocyte cultures markedly increases the production of basement membrane components. Such an effect may be usefully exploited to overcome the known weakness in the dermal-epidermal junction observed with current epidermal grafts.

- 10 Thus in accordance with another aspect of the present invention, we provide a wound dressing comprising;
- (a) a carrier layer having a wound facing non-adherent to cells surface having disposed thereon a biodegradable cell anchoring layer;
  - 15 (b) a layer of mammalian cells anchored to the cell anchoring layer.

The wound dressing of the present invention may be used in the treatment of a variety of wounds. The dressing of the invention  
20 is particularly suitable for treating partial thickness wound e.g. where the epidermis and possibly only part of the dermis is lost. Such wounds include skin graft donor sites, first or second degree burns, leg ulcers or pressure sores. The dressing may also be used for venous ulcers. In addition, the dressing of the present invention  
25 may find further use as part of a treatment for the chronic skin wounds that may develop following tumour excision and radiotherapy.

The wound dressing of the present invention maybe used in  
30 conjunction, e.g. simultaneously or sequentially, with other

treatments, for example, dermal replacement products such as **Dermagraft** (Trademark).

Thus in accordance with the present invention, we further  
5 provide a method of treating a skin trauma site on a mammalian patient comprising the step of;

applying to a patient a wound dressing which dressing comprises

- (a) a carrier layer having a wound-facing non-adherent to  
10 anchorage dependent cells surface and having disposed thereon a biodegradable cell anchoring layer;
- (b) a layer of mammalian cells anchored to the anchoring layer.

The wound dressing of the present invention may be prepared  
15 in accordance with standard cell culture techniques. The dressing may be placed in a suitable, preferably transparent, culture vessel with the cell anchoring layer face up. The vessel may be formed from suitable materials conventionally used in the manufacture of tissue culture vessels. High impact polystyrene is preferred. The  
20 dressing is then submerged in an aqueous medium comprising the cells and, if appropriate, the cell adhesion proteins. The medium utilised may be those commonly used in the field, e.g. dulbecco's modified eagle's medium (DMEM). The medium further comprises the usual nutrients, e.g. glucose, non-essential amino acids etc.  
25 Sufficient time is elapsed to allow the cells to become anchored to the cell anchoring layer and form a preferably sub-confluent layer.

It is preferred, however, to pretreat the carrier layer of the present invention e.g. by washing, with a solution of adhesion  
30 proteins such as FCS and then placing the dressing in a culture vessel comprising the aqueous media which includes nutrients, O<sub>2</sub>

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etc. and the cells. This accelerates the attachment of the cells by providing the cells with a ready-made layer i.e. the cell anchoring layer, on which to be anchored.

5           The dressing may then be removed from the culture vessel and applied to the wound of a patient, bringing the cell layer into contact with the wound site. The dressing may then be secured to the patient and left in place on the wound. Over a period of time, the cell anchoring layer which is suitably susceptible to enzymatic  
10 breakdown by e.g. proteases and heparinase present in the wound site, will degrade or breakdown, releasing the cell layer anchored thereto into the wound site. The non-adherent to cell layer disposed on the wound facing surface discourages re-attachment of the cells to wound dressing.

15

          If clinical concern dictates, proteases or heparinases may be added by the physician to the dressing once in place to accelerate the release of the cell layer.

20           In accordance with a further aspect of the present invention, we provide a method of preparing a wound dressing comprising the steps of;

- (a) forming a surface which is non-adherent to anchorage dependent cells on a wound facing surface of a carrier layer;
- 25           (b) forming a biodegradable cell anchoring layer on a non-adherent to anchorage dependent cells surface of a carrier layer;
- (c) culturing a carrier layer and biodegradable cell anchoring layer in the presence of mammalian cells.

30           The advantages of the wound dressing of the present invention include the ability to transfer cells from the dressing to the wound

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site more rapidly than with prior art devices. This is particularly desirable when rapid wound closure is desired. In use, the degradable layer breaks down releasing the cells into the wound site which are discouraged from attaching to the wound facing surface of the dressing by the non-adherent layer. The breakdown of the degradable layer will be further promoted by the presence of degradative enzymes known to be present in certain wound types. Thus the dressing can 'switch' from a cell binding state to a state in which the binding of cells to the dressing is discouraged.

10

The invention will now be illustrated by way of example only and with reference to the accompanying figures in which:

fig. 1a illustrates a photomicrograph of Scaber keratinocytes cells adhering to tissue culture plastic after four hours in culture.

fig. 1b illustrates photomicrograph of FCS pre-treated CMC films prepared as in example 1 below but without the addition of heparin.

20

fig. 1c illustrates a photomicrograph of Scaber cells cultured on the films of fig. 1b demonstrating that the cells do not adhere to the film and instead adhere to each other.

fig. 1d illustrates a photomicrograph of FCS pre-treated CMC/heparin films without cells prepared in accordance with example 1 below.

fig. 1e illustrates photomicrograph Scaber cells on the films of fig. 1d and demonstrating that the cells begin to adhere within 4 hours.

fig.2a illustrates a higher magnification photomicrograph view of fig.1a (mag x100)

- 5        fig.2b illustrates a high magnification photomicrograph view of fig.1c (mag x 100) demonstrating that the cells remain non-adherent and begin to clump.

- 10       fig.2c illustrates a high magnification view of fig.1e (mag x100), demonstrating the spreading of the applied cells over the film.

- 15       fig.3a to e illustrate photomicrographs of the views of fig.1a to e respectively after 16 hours from application of the cells to the film. fig.3c demonstrates that the cells remain non-adherent and form tighter clumps with increasing time. In contrast, fig.3e demonstrates the spreading of adherent Scaber cells upon the FCS pre-treated CMC/heparin films.

- 20       Fig.4 illustrates a photomicrograph of the view of fig.2a to c after 16 hours from the application of cells to the film.

Fig.5a illustrates a photomicrograph of Scaber cells grown upon tissue culture plastic for 7 days. The cells remain adherent.

- 25       Fig.5b illustrates a photomicrograph of FCS pre-treated CMC films without cells for 7 days.

- 30       Fig.5c illustrates a photmicrograph of cell seeded, FCS pretreated CMC films after 7 days, demonstrating the absence of adherent cells.



Fig.5d illustrates a photomicrograph of FCS pre-treated CMC/heparin films incubated without cells for 7 days

Fig.5e illustrates a photomicrograph of cell seeded FCS pre-treated CMC/heparin films after 7 days demonstrating that the adherent cells have detached.

Fig.6 illustrates a co-culture of Human foreskin fibroblasts and a non-cell seeded, FCS pre-treated CMC heparin film incubated for 7 days. This photomicrograph demonstrates that the cells remain viable and adherent to the plastic, providing evidence that the cell detachment shown in fig.5e is not the result of cellular toxicity.

#### Example 1

Carboxymethyl cellulose (Blanose™, Aqualon), was dissolved as a 1% aqueous solution. EGDGE (20% w/w, Aldrich) was added and the solution mixed briefly using a magnetic stirrer. The resulting mixture was allowed to stand at 37°C for 16 hours. Opsite IV 3000 (Smith&Nephew) polyurethane film was exposed to nitrogen plasma (1 minute; 100W; Chamber pressure 0.1 to 0.2 mbar; using a PT7300 etcher) and promptly covered with a thin coat of EGDGE/CMC reaction mix (approx. 0.05ml/cm<sup>2</sup>). An aqueous solution of heparin (10mg/ml; 0.1ml/cm<sup>2</sup>) was then sprayed on top of the CMC/EGDGE coating and the resulting material dried at 60°C for 5 hours. The resulting films were then sterilised and stored dry.

The films were then immersed in Foetal Calf Serum (40%w/w, GIBCO) in phosphate buffer saline (PBS) for 16 hours at 37°C. The films were then washed twice with PBS and human keratinocytes suspended in serum free Keratinocyte basal medium (KBM) supplemented with Keratinocyte growth medium (KGM) growth

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additives (available from Clonetics, Walkersville, Maryland USA). As a control, aliquots of the suspended cells were added to the wells of a tissue culture plate (Falcon 3043 tissue culture plate). Cells adhered to the film and plate within 4 to 16 hours with a favourable level of spread and adherence after 1 to 2 days. This is illustrated in fig.1 to 4. Following subsequent in vitro culture, the cells detached from the film and were released into the medium (see fig.5). Released cells formed clumps over the subsequent 7 day culture period. In contrast, cells added to tissue culture plastic adhered within 4 to 16 hours but remained adherent over the next 7 days (see fig.5a)

Cell detachment from the FCS pre-treated CMC/heparin films was not a consequence of toxicity because if cells were cultured in tissue wells that contained a FCS pre-treated CMC/heparin film the cells remained adherent upon the culture plastic for the entire 7 day period (fig.6).

### Example 2

#### 20 Preparation of methyl cellulose/EGDGE/polylysine films

Carbonate buffer, pH 11, was prepared as follows:

Solution A = 10.6g  $\text{Na}_2\text{CO}_3$  in  $\text{H}_2\text{O}$  (500ml)

Solution B = 8.4g  $\text{NaHCO}_3$  in  $\text{H}_2\text{O}$  (500ml)

25 Solution C = 330ml Solution A + 170ml Solution B adjusted to pH 11 with NaOH.

Methyl cellulose (1g, Aldrich Chemicals) was dissolved in buffer (solution C) (100ml, pH 11; stir for 16 hours at room temperature). A hydrophilic polyurethane (PU) sheet (IV3000, Smith & Nephew) and was treated with Corona discharge to increase its hydrophilicity (2

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meters/min, 0.3 kW, Aluminium trough electrode; Sherman Instruments). Methyl Cellulose solution (10g) was mixed with Ethylene Glycol DiGlycidyl Ether (EGDGE, 10 $\mu$ l) and the resulting solution spread on the polyurethane film using a spreading block to

- 5 give a methyl cellulose/EGDGE film of 18/1000 inch thick. The spreaded PU film was then heated (60°C, 1 hour). Polylysine in aqueous solution (1mg/10cm<sup>2</sup>, Sigma) was sprayed onto the spreaded PU film and dried for 2 hours at 60°C. The films were washed twice with DMEM and twice in serum-free media (Gibco).
- 10 Trypinised cells (primary human keratinocytes) were resuspended in serum-free media and added to the films. Cells began to adhere after 4 to 16 hours.

#### Example 3

- 15 FCS pre-treated heparinised/ agarose film was prepared in place of CMC of example 1. Cells bound within 4 to 16 hours and detached within 7 days.

#### Example 4

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The film of example 3 was prepared substituting Fucoidin (Sigma) for the heparin.

#### Example 5

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The film of example 4 was prepared substituting gelatin (5mg/ml, Sigma) for fucoidin.

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**CLAIMS**

1. A wound dressing comprising a carrier layer having a wound-facing surface, said surface being non-adherent to anchorage-dependent cells and having disposed thereon a biodegradable cell anchoring layer.
2. The wound dressing of claim 1 wherein the carrier layer comprises a polymeric material.
3. The wound dressing of claim 2 wherein the material is a cross-linked hydroxyalkyl cellulose, a cross-linked carboxyalkyl cellulose, a polyvinyl alcohol or an agarose.
4. The wound dressing of claim 1 wherein the carrier layer comprises a material adherent to anchorage dependent cells and treated on the wound facing surface thereof to be non-adherent to cells.
5. The wound dressing of claim 4 wherein the adherent material comprises a polymer selected from a group consisting of; polyhydroxyethylmethacrylic acids, cross-linked polyvinylalcohols, polyacrylic acids cross-linked with trialkylsucrose, polyvinylpyrrolidones, polyetherpolyesters, polyetherpolyamides, polycrylamides, polyethylene oxide, polyurethanes and ethylene-vinyl acetate copolymers.
6. The wound dressing of claim 4 or 5 wherein the wound facing surface is treated with a phosphocholine, a silicone, a polyethylene glycol or a polytetrafluoroethylene.
7. A wound dressing according to any one preceding claim wherein the biodegradable cell anchoring layer comprises a polyanion moiety.
8. The wound dressing of claim 7 wherein the polyanion moiety has anchored thereto a cell adhesion protein.

9. The wound dressing of claim 7 or 8 wherein the polyanion is a heparin, an inositol phosphate, fucoidin, syndecan, betaglycan, perlecan, dextran sulphate, pentosan, mesoglycan or polyvinyl sulphate.
10. The wound dressing of any of claims 1 to 6 wherein the biodegradable cell anchoring layer comprises a polypeptide.
11. The wound dressing of claim 10 wherein the polypeptide is polylysine.
12. The wound dressing of any preceding claim wherein the cell anchoring layer has anchored thereto mammalian cells which form a cell layer.
13. The wound dressing of claim 12 wherein the cell layer comprises either keratinocytes or fibroblasts
14. The wound dressing of claim 12 wherein the cell layer comprises both keratinocytes and fibroblasts.
15. The wound dressing of claims 12 to 14 wherein the cell layer comprises either autologous cells or allogenic cells.
16. The wound dressing of claims 12 to 14 wherein the cell layer comprises both autologous and allogenic cells.
17. A cell culture system comprising;
- (a) a wound dressing comprising a carrier layer having a wound-facing surface, said surface being non-adherent to anchorage dependent cells and having disposed thereon a biodegradable cell anchoring layer and

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- (b) a vessel having interior and exterior surfaces for containing a liquid culture medium for culturing cells and the dressing.

- 5 18. A method of treating a skin trauma site on a mammalian patient comprising the step of applying to a patient a wound dressing which dressing comprises;

10 (a) a carrier layer comprising a wound surface which is non-adherent to anchorage dependent cells and having disposed thereon a biodegradable cell anchoring layer;

15 (b) a layer of mammalian cells anchored to the anchoring layer.

19. A method of preparing a wound dressing comprising the steps of;

20 (a) obtaining a surface which is non-adherent to anchorage dependent cells on a wound facing surface of a carrier layer;

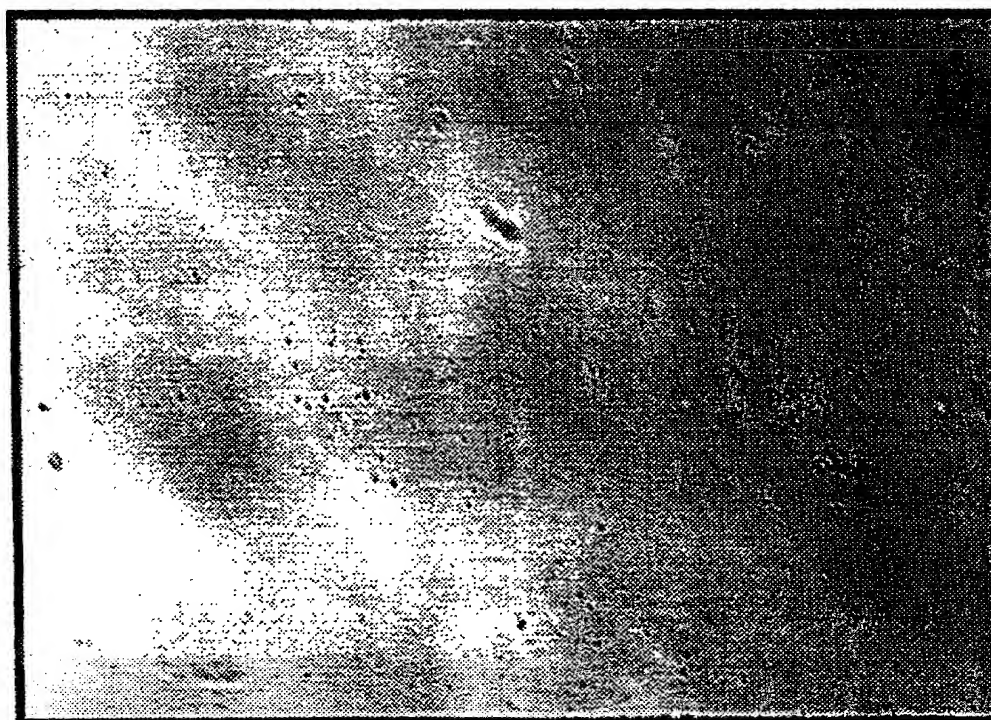
(b) forming a biodegradable cell anchoring layer on a non-adherent to anchorage dependent cells surface of a carrier layer;

25 (c) culturing a carrier layer which comprises a non-adherent to anchorage dependent cell surface and biodegradable cell anchoring layer in the presence of mammalian cells.

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*FIG. 1a.*

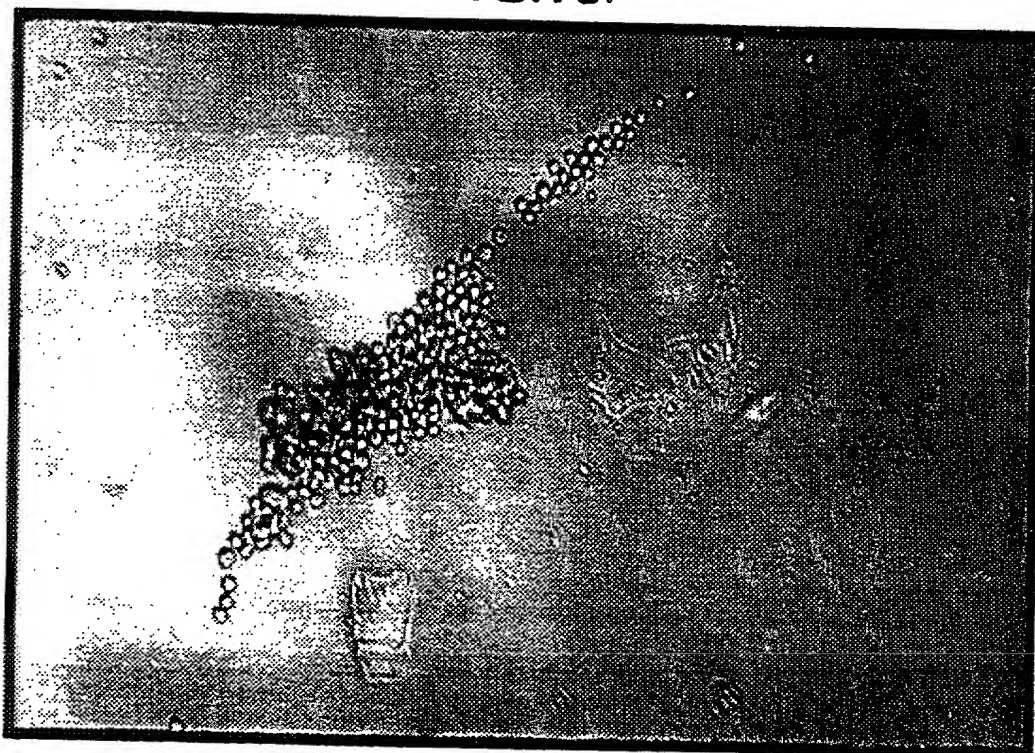


*FIG. 1b.*

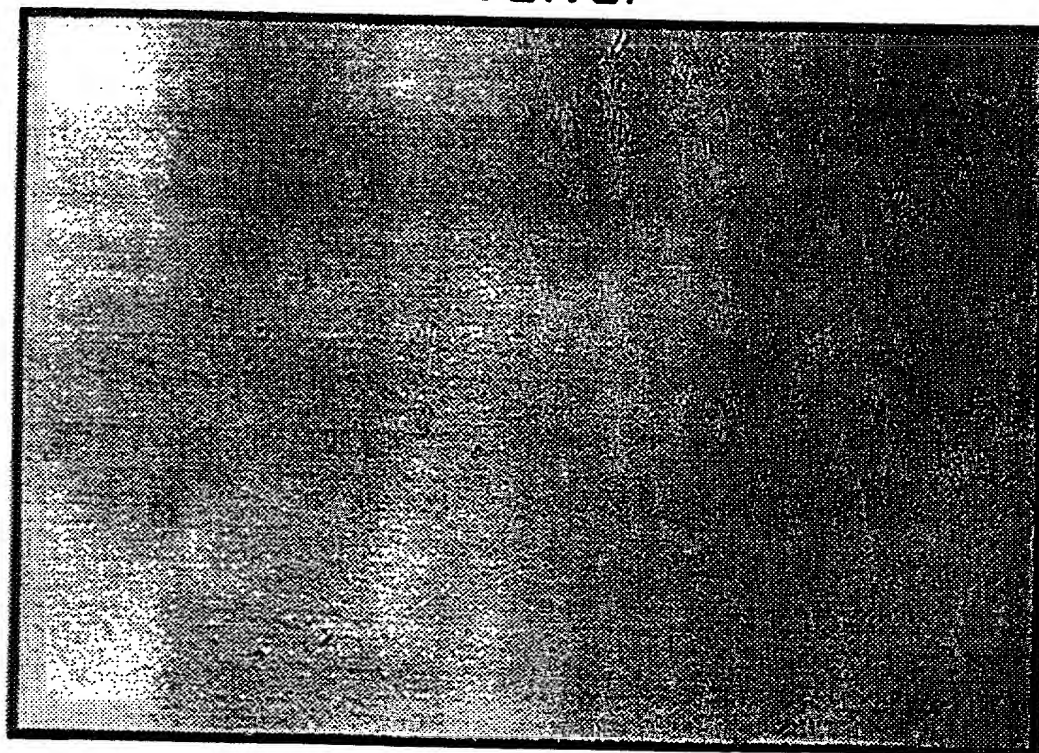


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*FIG.1c.*

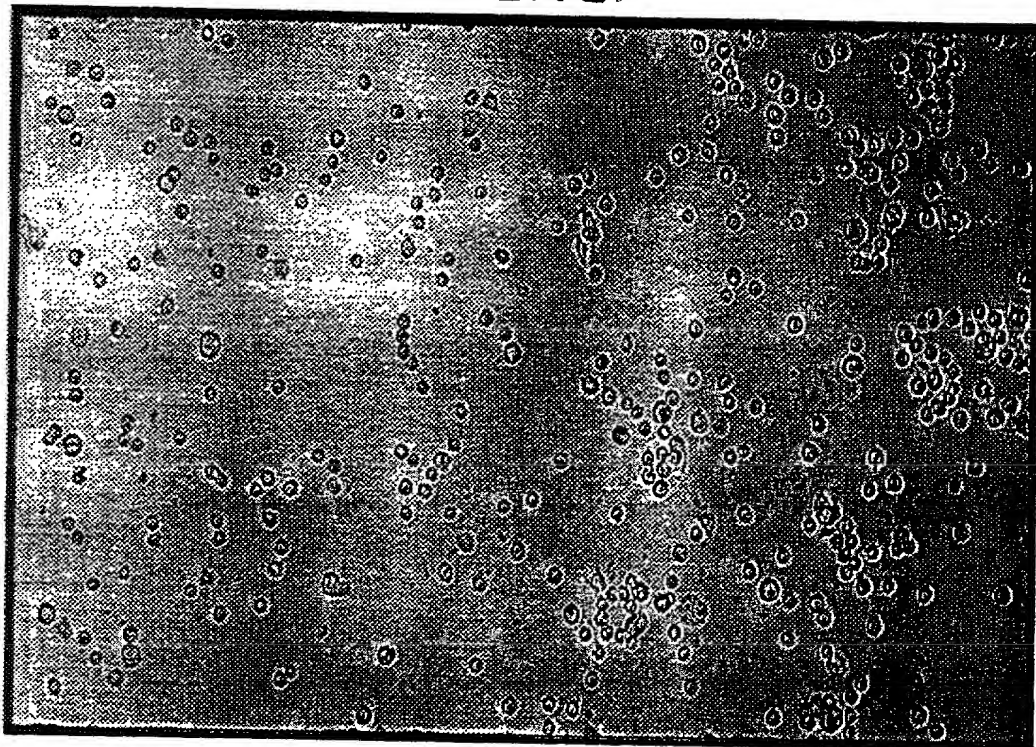


*FIG.1d.*

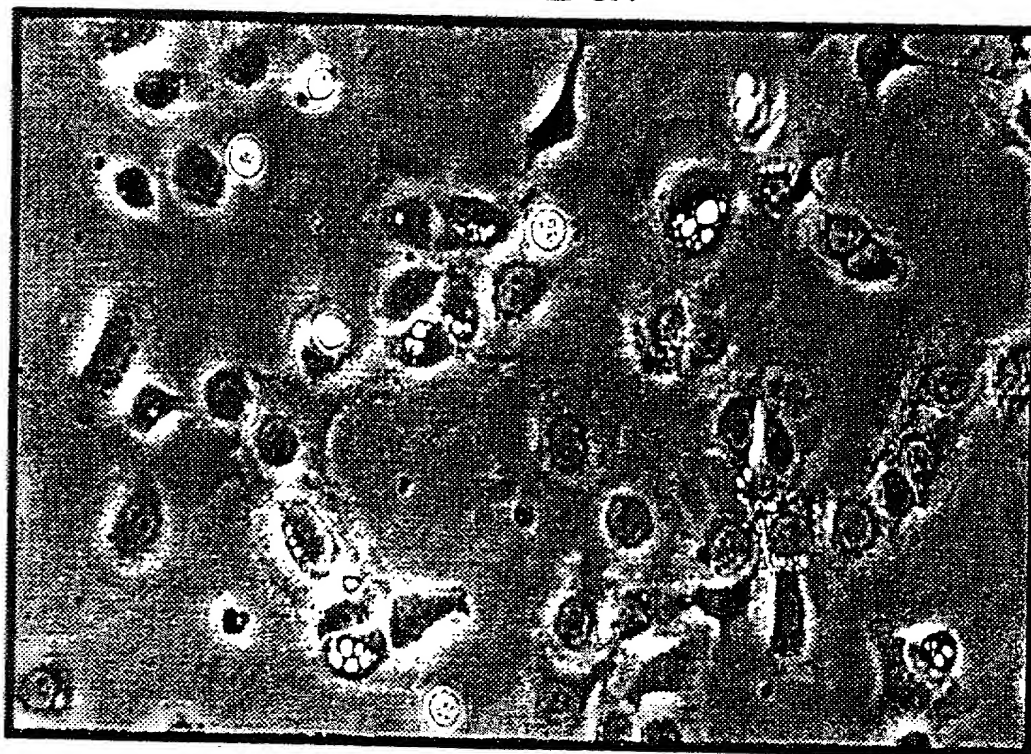




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*FIG. 1e.*



*FIG. 2a.*



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FIG. 2b.

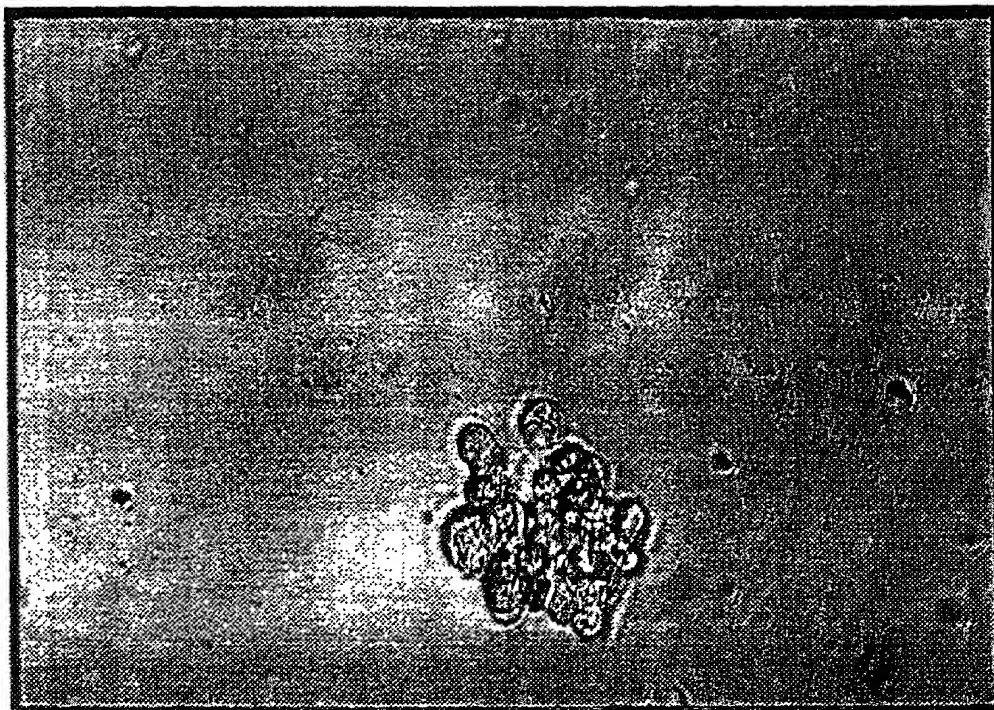
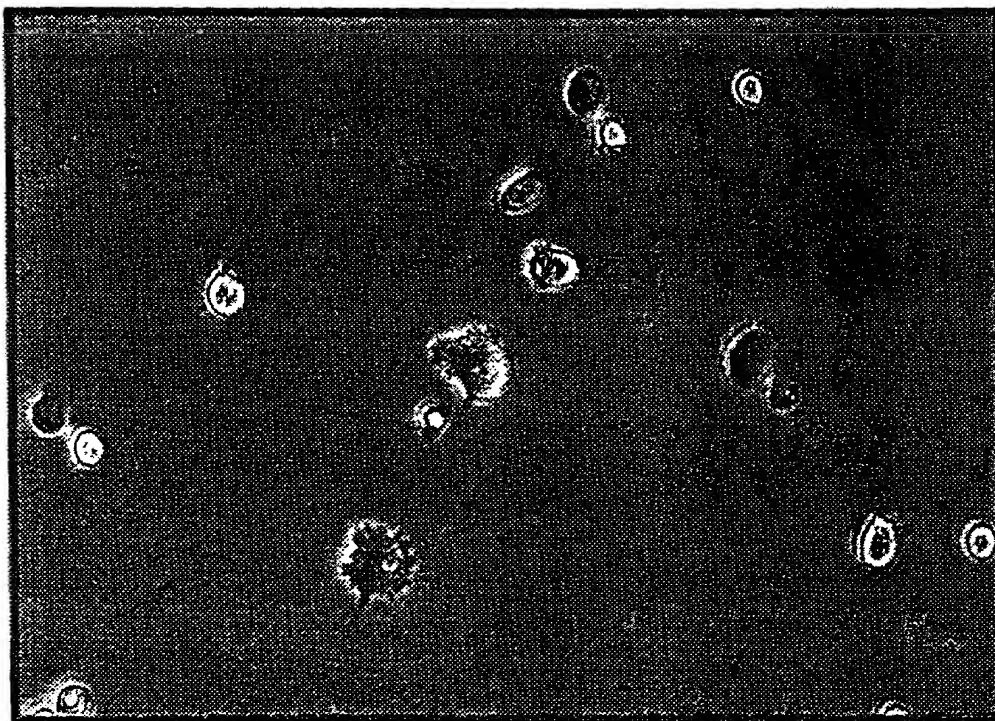
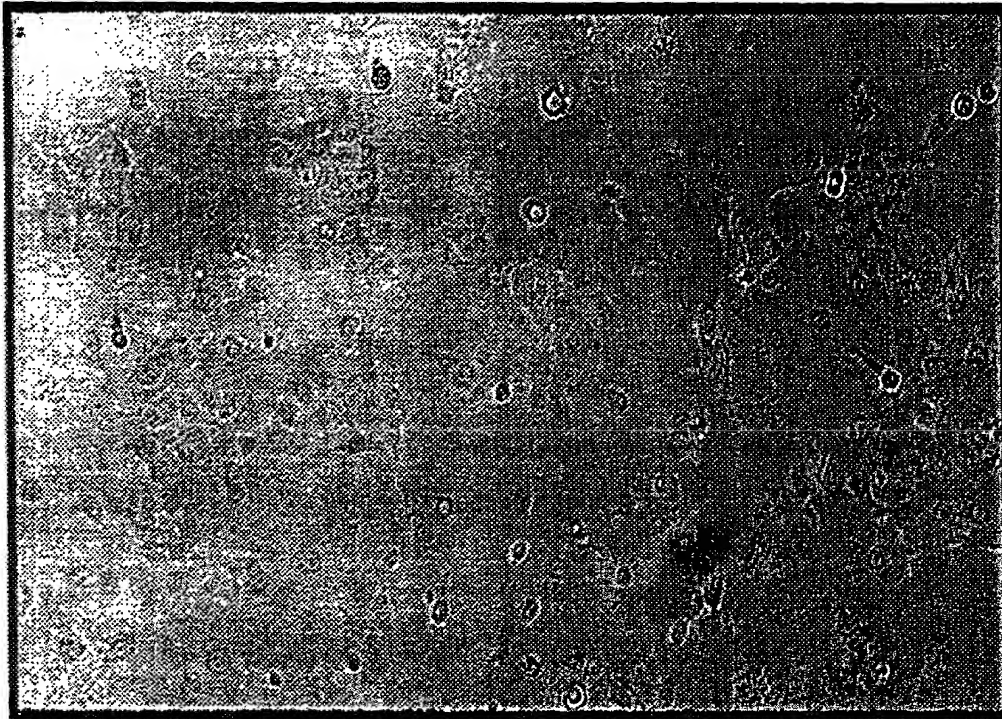


FIG. 2c.



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*FIG. 3a.*

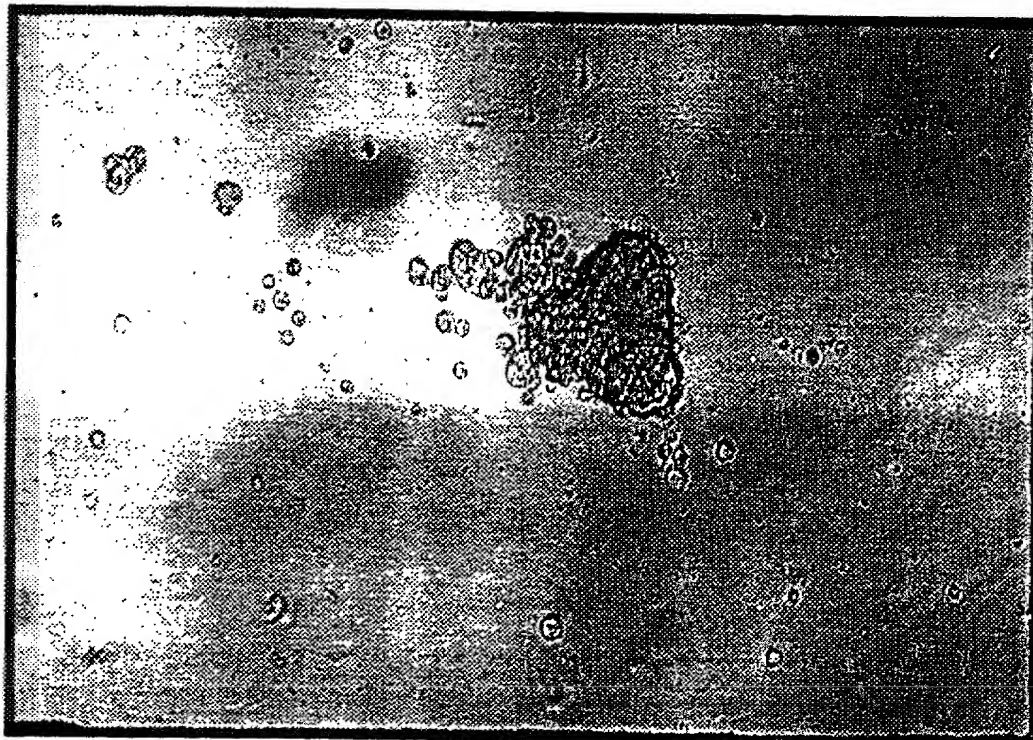


*FIG. 3b.*

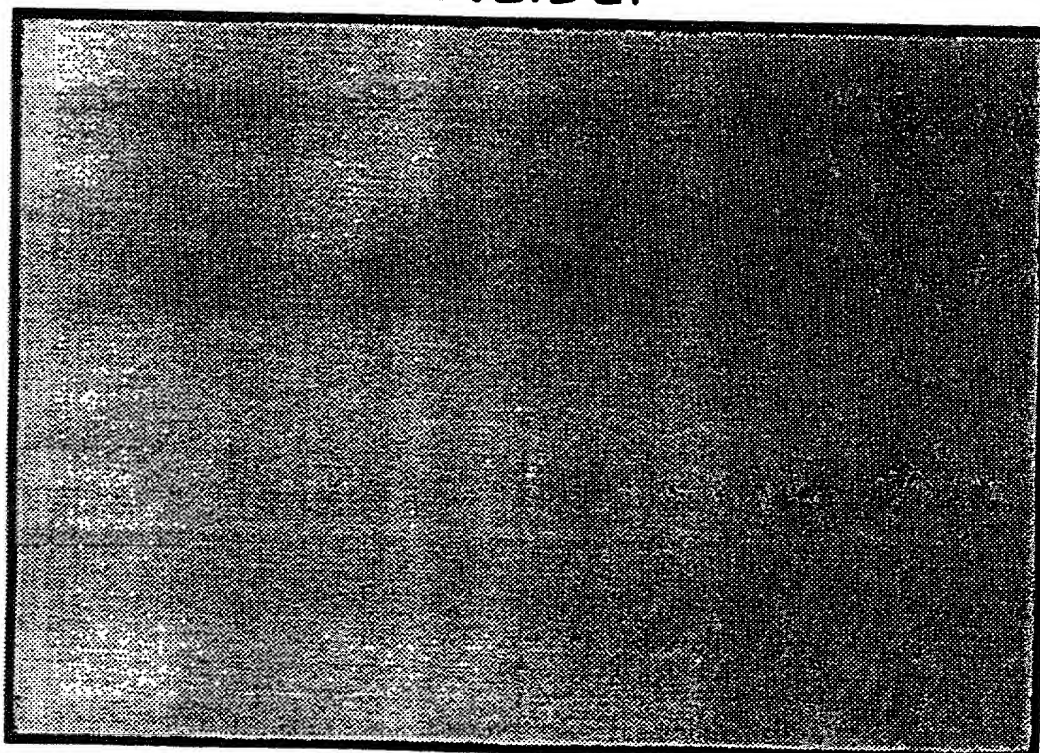




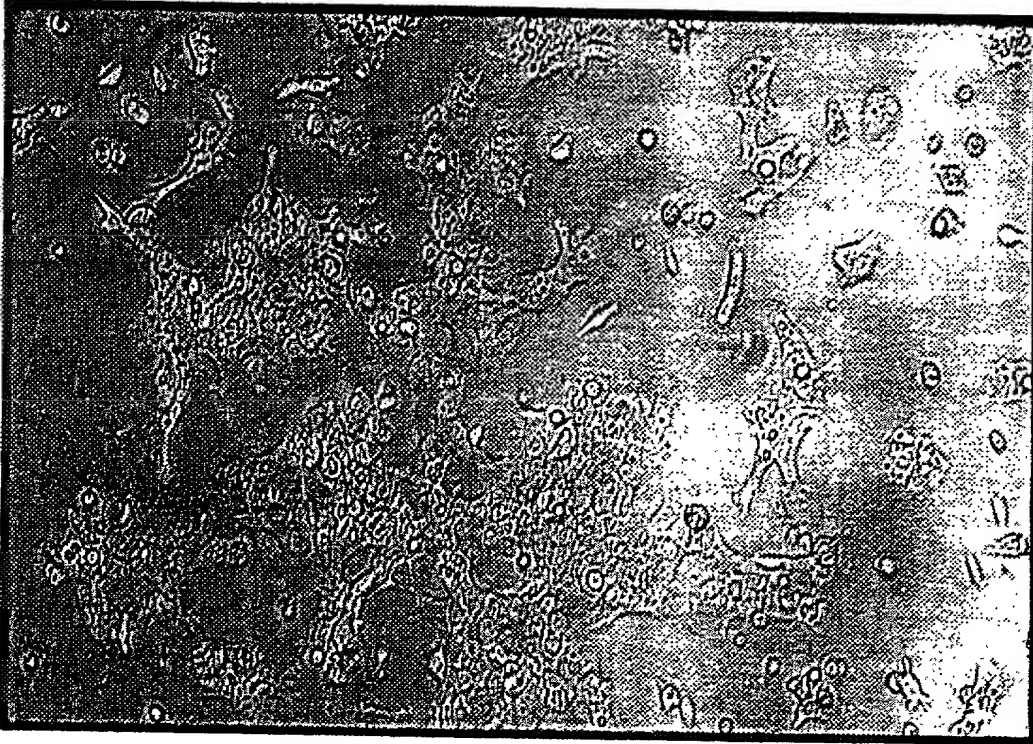
6/11  
*FIG. 3c.*



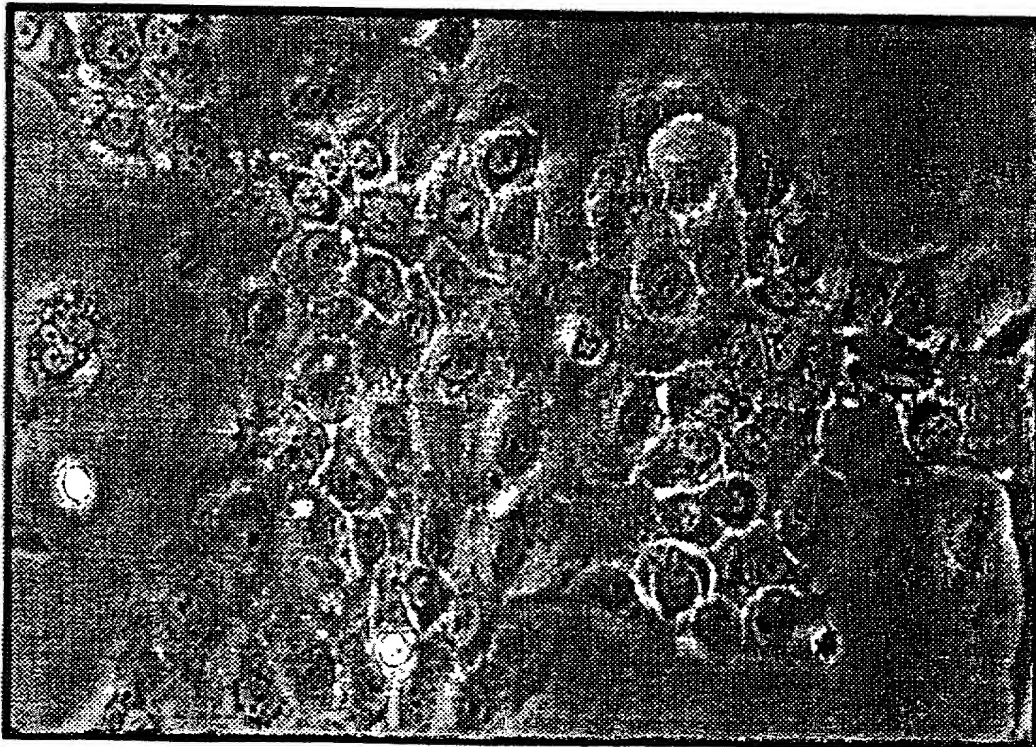
*FIG. 3d.*



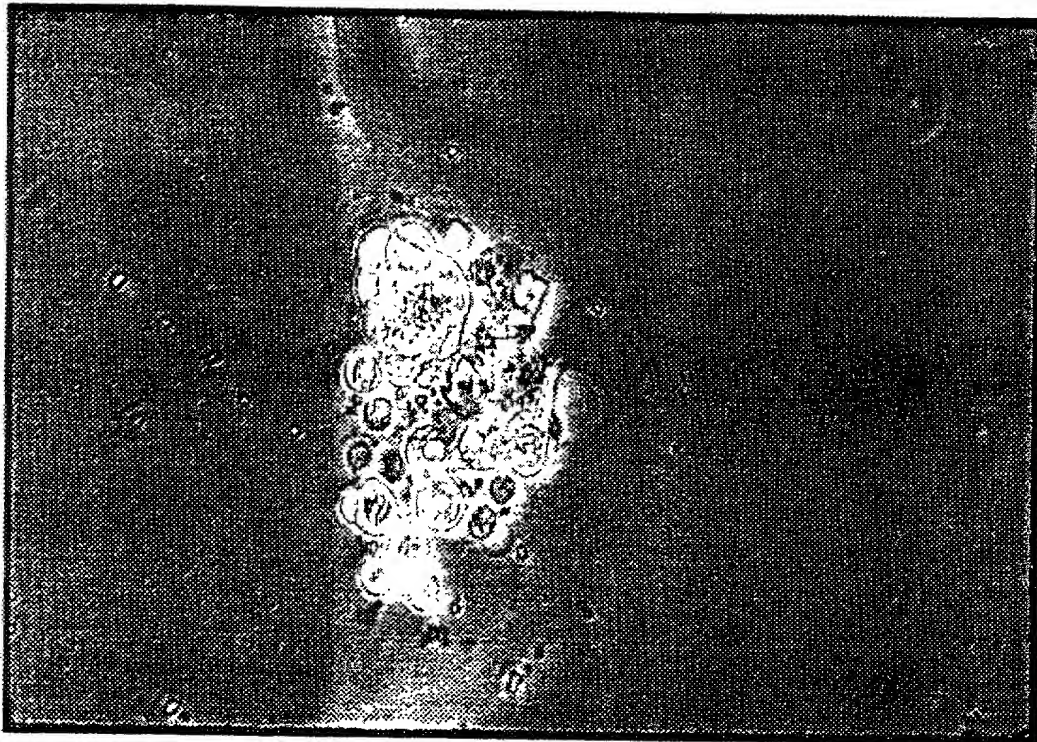
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*FIG. 3e.*



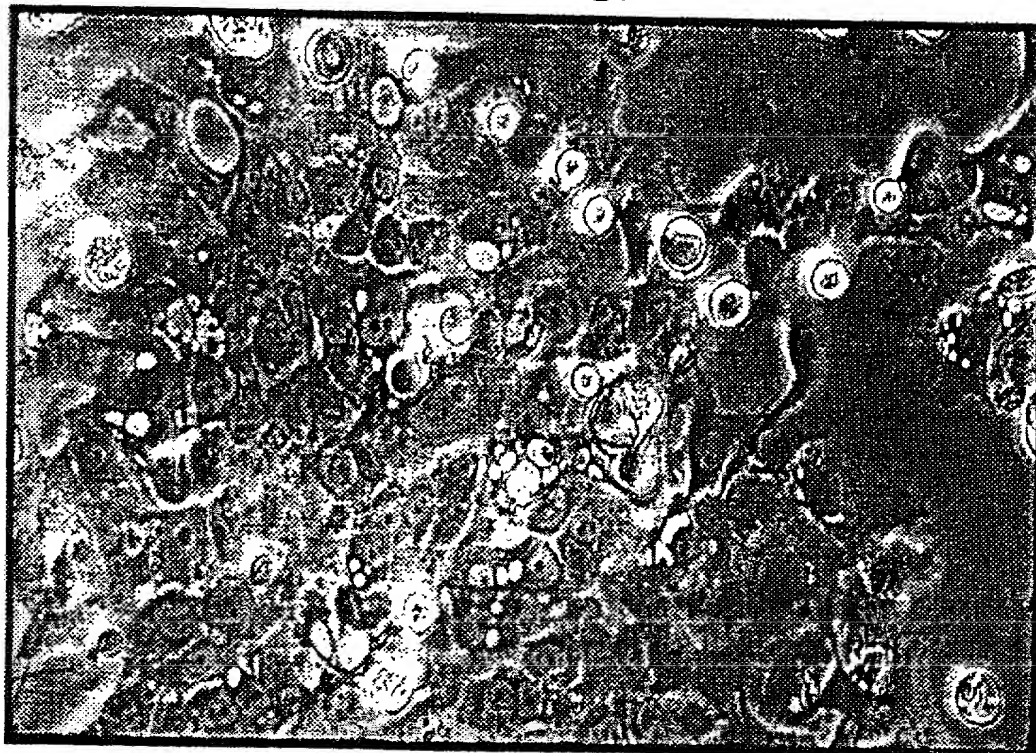
*FIG. 4a.*



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*FIG. 4b.*



*FIG. 4c.*

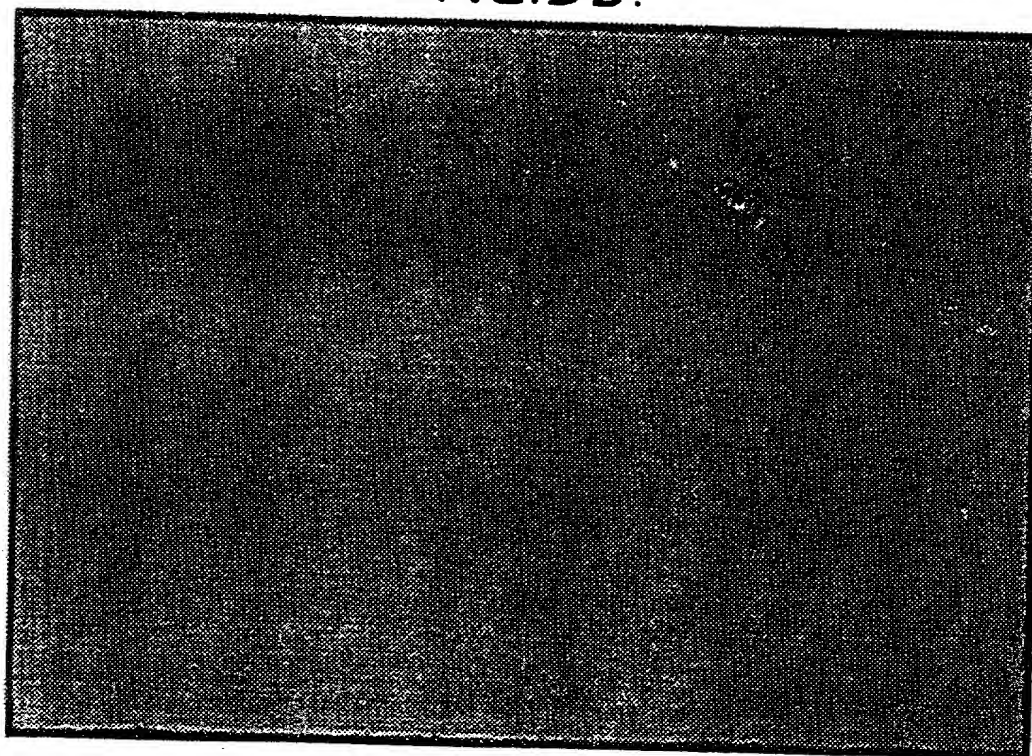




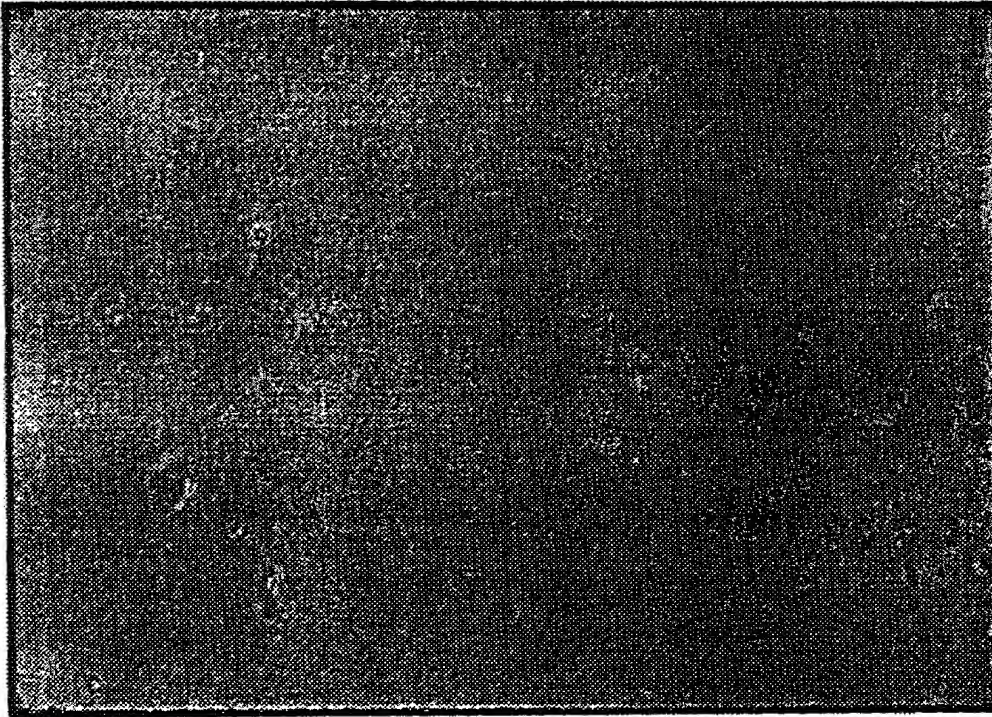
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*FIG. 5a.*



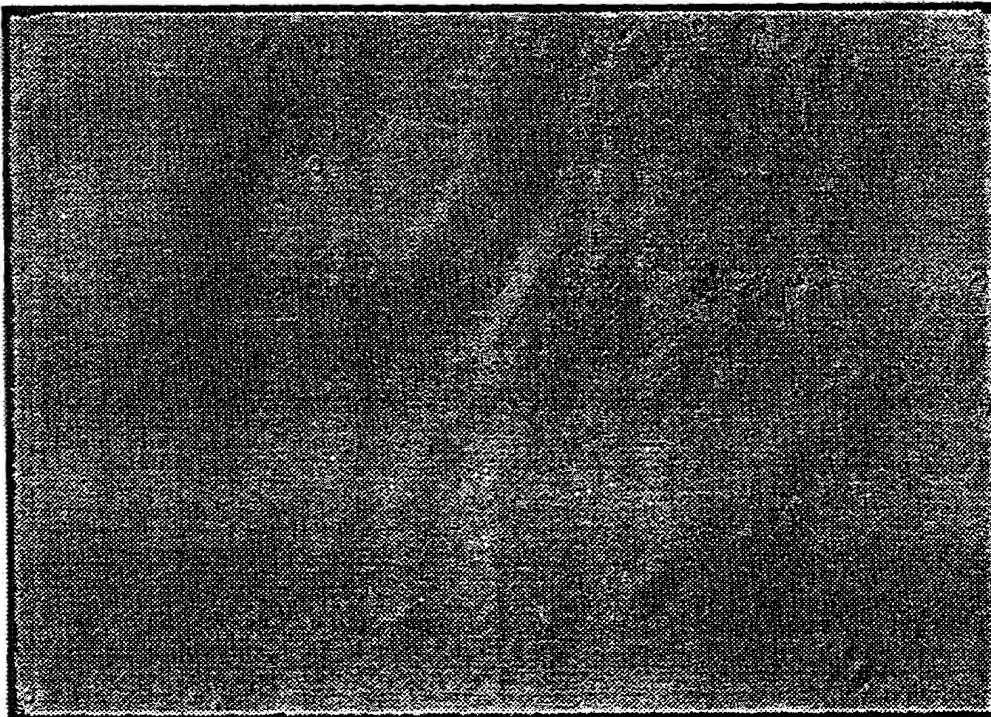
*FIG. 5b.*



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*FIG. 5c.*



*FIG. 5d.*





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FIG. 5e.

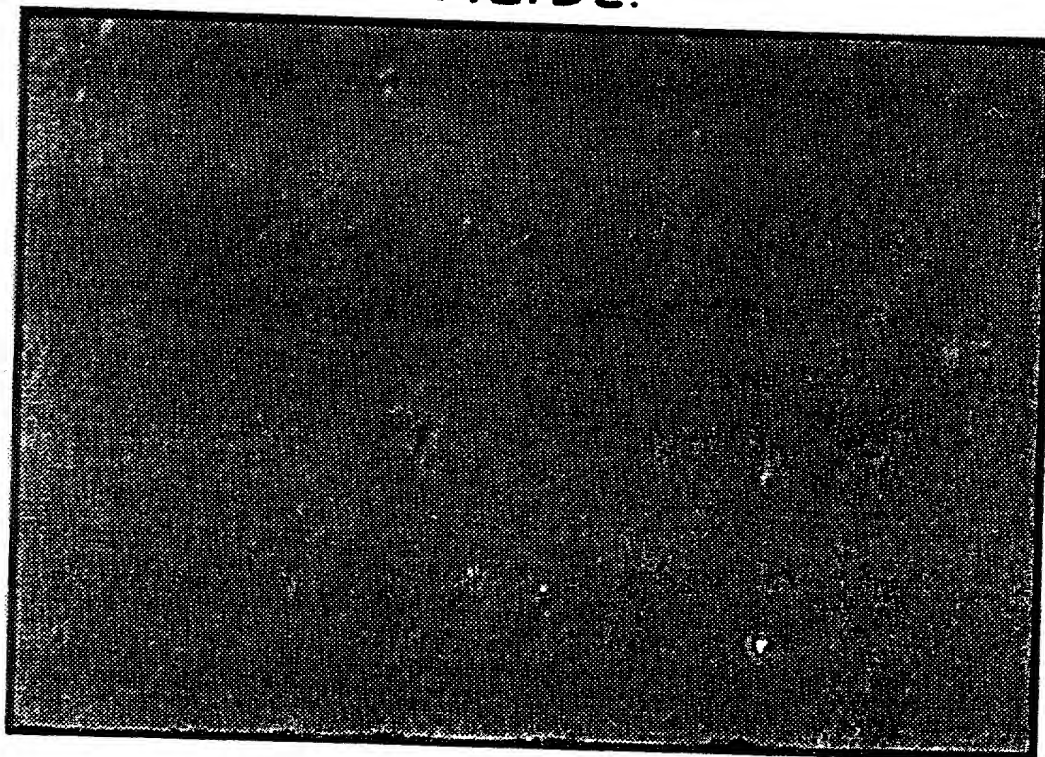
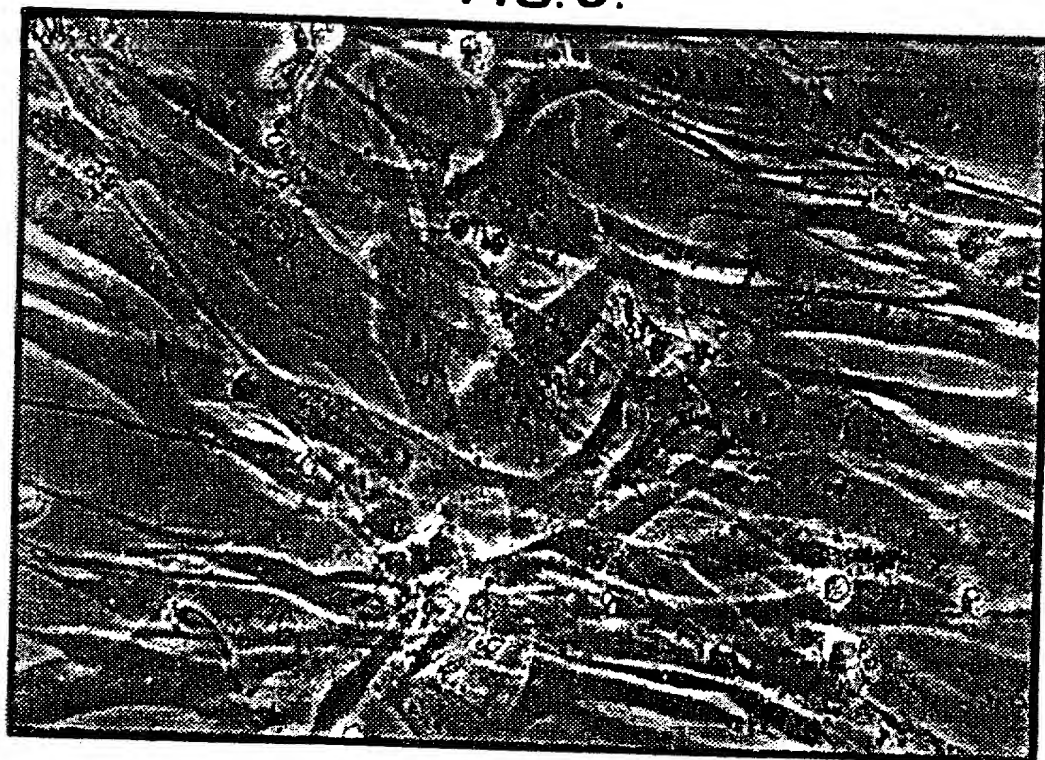


FIG. 6.



## DECLARATION FOR USA PATENT APPLICATION

(including Design and National Stage PCT)

Attorney's Docket ID: \_\_\_\_\_

As a below named inventor, I hereby declare that:

My residence, post office address and citizenship are as stated below adjacent to my name. I believe I am the original, first and sole inventor (if only one name is listed below) or an original, first and joint inventor (if plural names are listed below) of the subject matter which is claimed and for which a patent is sought on the invention entitled Cell Culture Products

\_\_\_\_\_, the specification of which \_\_\_\_\_ is attached hereto. (or)

☒ was filed on 26 June 1998, [ ] and was amended on \_\_\_\_\_

[ ] as U.S. Application No. \_\_\_\_\_ or

[X] as International PCT Application No. GB98/01882

I hereby state that I have reviewed and understand the contents of the above-identified specification, including the claims, as amended by any amendment referred to above. I acknowledge the duty to disclose information which is material to patentability as defined in Title 37, Code of Federal Regulations, § 1.56.

I hereby claim foreign priority benefits under Title 35, United States Code, § 119 (a) - (d) or §365 (b) of any foreign application(s) for patent or inventor's certificate, or §365 (a) of any PCT International application which designated at least one country other than the United States of America, listed below and have also identified below, where priority is not claimed, any foreign application for patent or inventor's certificate, or any PCT International application, having a filing date before that of the application on which priority is claimed:

Prior Foreign Application(s) (\_\_\_\_\_) ADDITIONAL APPLICATIONS IDENTIFIED ON ATTACHED SHEET:

Number	Country	Day/Month/Year Filed	Priority Not Claimed
<u>9713406.8</u>	<u>GB</u>	<u>26 June 1997</u>	_____
<u>9725209.2</u>	<u>GB</u>	<u>28 November 1997</u>	_____

I hereby claim the benefit under Title 35, United States Code, § 120 of any United States application(s), or §365(c) of any PCT International application designating the U.S., listed below; and insofar as the subject matter of each claim of this application is not disclosed in the prior United States or PCT International application in the manner provided by the first paragraph of Title 35, United States Code, § 112, I acknowledge the duty to disclose information which is material to patentability as defined in Title 37, Code of Federal Regulations § 1.56 which became available between the filing date of the prior application and the national or PCT International filing date of this application. (\_\_\_\_\_) ADDITIONAL APPLICATIONS IDENTIFIED ON ATTACHED SHEET:

Application Serial No.	Day/Month/Year Filed	Status - patented, pending, abandoned
_____	_____	_____
_____	_____	_____

I hereby appoint the practitioners of LARSON & TAYLOR associated with the Customer Number provided below to prosecute this application and to transact all business in the Patent and Trademark Office connected therewith, and direct that all correspondence be addressed to that Customer Number.

CUSTOMER NUMBER: 000881

Direct all telephone calls to \_\_\_\_\_, at TEL (703) 739-4900 (Fax: 703-739-9577)

I hereby declare that all statements made herein of my own knowledge are true and that all statements made on information and belief are believed to be true; and further that these statements were made with the knowledge that willful false statements and the like so made are punishable by fine or imprisonment, or both, under § 1001 of Title 18 of the United States Code and that such willful false statements may jeopardize the validity of the application or any patent issued thereon.

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Residence - City, State/Country (if different from P.O. address)	_____		
SIGN AND DATE HERE: Inventor's Signature:	<u>[Signature]</u>	Date:	<u>20/01/00</u>

Full Name of Fourth Joint Inventor, if any	<u>John MALTMAN</u>	Citizenship	<u>United Kingdom</u>
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Residence - City, State/Country (if different from P.O. address)	_____		
SIGN AND DATE HERE: Inventor's Signature:	<u>[Signature]</u>	Date:	<u>19/01/2000</u>

SEE ATTACHED SHEET FOR SIMILAR INFORMATION AND SIGNATURE FOR ADDITIONAL JOINT INVENTORS.  
LARSON & TAYLOR, 1199 North Fairfax Street, Suite 900, Alexandria Virginia 22314

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**DECLARATION FOR USA PATENT APPLICATION**  
(including Design and PCT)

**ADDITIONAL INFORMATION SHEET**  
(use as required)

I hereby claim the benefit under Title 35, United States Code § 119 (e) of any United States PROVISIONAL application(s) listed below.

Application No.	Day/Month/Year Filed
_____	_____
_____	_____

Additional Prior Foreign Application(s):

Number	Country	Day/Month/Year Filed	Priority Not Claimed
_____	_____	_____	_____
_____	_____	_____	_____

Additional 35 U.S.C. § 120 applications:

Application Serial No.	Day/Month/Year Filed	Status — patented, pending, abandoned
_____	_____	_____
_____	_____	_____

Additional Joint Inventors:

Full Name of Fifth Joint Inventor, if any	<u>Sharon Dawn MALTMAN</u>	Citizenship	<u>United Kingdom</u>
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SIGN AND	
DATE HERE: Inventor's Signature: <u>S. D. Maltman.</u>	Date: <u>18/01/00.</u>

Full Name of Sixth Joint Inventor, if any	Citizenship
Full Post Office Address	
Residence - City, State/Country (if different from P.O. address)	
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DATE HERE: Inventor's Signature:	Date:

Full Name of Seventh Joint Inventor, if any	Citizenship
Full Post Office Address	
Residence - City, State/Country (if different from P.O. address)	
SIGN AND	
DATE HERE: Inventor's Signature:	Date:

Full Name of Eighth Joint Inventor, if any	Citizenship
Full Post Office Address	
Residence - City, State/Country (if different from P.O. address)	
SIGN AND	
DATE HERE: Inventor's Signature:	Date: